AMENDMENTS TO THE SPECIFICATION

In the specification of the Application, please amend paragraph 0021 as hereinafter indicated.

[0021] A main magnetic field shield coil assembly 30 generates a magnetic field that opposes the field generated by the superconducting magnet coils 22. A toroidal vacuum vessel 32 includes a cylindrical member 34 that defines the patient bore 24 and extends parallel to a longitudinal axis 36. The patient bore [[18]] 24 has [[a]] an RF coil assembly 42 mounted therein. The RF coil assembly 42 includes the primary RF coil or imaging coil 12 and [[a]] an RF shield 44. On a first exterior side 45 of the cylindrical member 34 is a magnetic gradient coil assembly 47.

Please also amend paragraph 0033 in the specification as hereinafter indicated.

[0033] The capacitors 102, within each capacitor grouping, are "spread out" ~~longitudinally and parallel to~~ along the longitudinal axis 36 such that the coverage area 103 of the capacitors 102 has a width W that is approximately greater than 5.0cm, which is also greater than that of prior art body coils. The width of the groupings 104 and 106 may be approximately equal, as shown, or may be different. Increased width of the capacitor groupings 98 further distributes RF currents and reduces generation of E-fields. Also, the capacitors 102 are positioned farther away from the patient bore 24, which decreases size of the local E-fields associated therewith. Wider end rings 52 exhibit lower inductance between the capacitors 98, which enables higher capacitance in the endrings 52.

Lastly, in the specification, please also amend paragraphs 0035 and 0036 as hereinafter indicated.

[0035] The center ring 53 is coupled to a ground reference 110, which has low impedance, such that the center ring 53 is effectively "shorted" to the ground reference 110. The center ring 53 includes a series of capacitors 112, which are coupled between the legs 86. As shown in Figure 3, [[The]] the capacitors 112 are ~~adjacently~~ coupled together via connections 113 therebetween. [[As]] Configured as such, the center ring 53, like the end rings 52, is ~~circumferentially conductive~~ substantially centered around a common axis, as is shown in Figures 1 and 2. The capacitors 112 have low impedance at frequency levels of approximately greater than or equal to 120MHz. The center ring 53 may have any number of capacitors. Shorting the center ring 53 ensures symmetry of the imaging coil 12 end-to-end. Shorting the center ring 53 also allows for use of balun-less drive cables between the splitter 72 and the end rings 52.

[0036] Each ~~receiver~~ decoupling circuit 74 has associated ~~adjacent~~ capacitors, which are generally coupled to ~~receiver~~ decoupling circuits on an opposing end ring. For example, as shown in Figure 3, ~~receiver~~ decoupling circuit 114, on the forward end ring 88, has ~~adjacent~~ associated capacitors 116, which are coupled to ~~receiver~~ decoupling circuits 118.